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	Division	Departments of Biology, Electrical and Computer Engineering, and Physics
	Organization	Center for the Interdisciplinary Research on Complex Systems, Northeastern University
	Address	134 Mugar Life Science Building, 360 Huntington Avenue, Boston, MA, 02115, USA
	Email	dagmar@northeastern.edu
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Keywords (separated by '-')	Human motor control - Motor learning - Neuromotor noise - Variability - Stability - Predictability - Tool use	

Human Control of Interactions with Objects – Variability, Stability and Predictability

Dagmar Sternad

Abstract How do humans control their actions and interactions with the physical world? How do we learn to throw a ball or drink a glass of wine without spilling? Compared to robots human dexterity remains astonishing, especially as slow neural transmission and high levels of noise seem to plague the biological system. What are human control strategies that skillfully navigate, overcome, and even exploit these disadvantages? To gain insight we propose an approach that centers on how task dynamics constrain and enable (inter-)actions. Agnostic about details of the controller, we start with a physical model of the task that permits full understanding of the solution space. Rendering the task in a virtual environment, we examine how humans learn solutions that meet complex task demands. Central to numerous skills is redundancy that allows exploration and exploitation of subsets of solutions. We hypothesize that humans seek solutions that are stable to perturbations to make their intrinsic noise matter less. With fewer corrections necessary, the system is less afflicted by long delays in the feedback loop. Three experimental paradigms exemplify our approach: throwing a ball to a target, rhythmic bouncing of a ball, and carrying a complex object. For the throwing task, results show that actors are sensitive to the error-tolerance afforded by the task. In rhythmic ball bouncing, subjects exploit the dynamic stability of the paddle-ball system. When manipulating a “glass of wine”, subjects learn strategies that make the hand-object interactions more predictable. These findings set the stage for developing propositions about the controller: We posit that complex actions are generated with dynamic primitives, modules with attractor stability that are less sensitive to delays and noise in the neuro-mechanical system.

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D. Sternad (✉)

Departments of Biology, Electrical and Computer Engineering, and Physics, Center for the Interdisciplinary Research on Complex Systems, Northeastern University, 134 Mugar Life Science Building, 360 Huntington Avenue, Boston, MA 02115, USA
e-mail: dagmar@northeastern.edu

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1 Introduction

Imagine a dancer, perhaps Rudolf Nureyev or Margaret Fonteyn, both legends in classical ballet: we can only marvel at how they are in complete control of their body, combining extraordinary flexibility and strength with technical difficulty and elegance. And yet, I submit that Evgenia Kanaeva, two-times all-around Olympic champion in rhythmic gymnastics, equals, if not surpasses their level of skill: Not only does she move her lithe body with perfection and grace, she also plays with numerous objects: she throws, catches and bounces a ball, she rolls and swivels a hoop, and sets a 6 m-long ribbon into smooth spirals with the most exquisite movements of her hands and fingers – and yes, sometimes also using her arms, shoulders, or her legs and feet. Her magical actions and interactions with objects arguably represent the pinnacle of human motor control.

How do humans act and interact with objects and tools? After all, tool use is what gave humans their evolutionary advantage over other mammals. In robotics, manipulation of tools has clearly been one of the primary motivations to develop robots, going back to the first industrial robots designed to automate repetitive tasks such as placing parts. However, these actions lack the dexterity that not only elite performers, but all healthy humans display. Opening a bottle of wine with a corkscrew or eating escargot with a fork and tongs are skills that require subtle interactions with complex tools and objects. How do humans control these actions and interactions?

Research in motor neuroscience has only arrived at limited answers. To assure experimental control and rigor, computational research has confined itself to simple laboratory tasks, most commonly reaching to a point target, while restricting arm movements to two joints moving in the horizontal plane [57, 58]. Research on sequence learning has typically been limited to finger presses evaluated with simple discrete metrics of timing and serial errors [43, 82]. Grasping has been reduced to isometric finger presses with predetermined contact points to analyze contact forces [37, 83]. The obvious benefit of such simplifications is that the data are accessible and tractable for testing theory-derived hypotheses. Over the past 20 years, numerous studies in computational neuroscience have embraced control-theoretical concepts, such as Kalman filters [39], Bayesian multi-sensory integration [2, 81], and optimal feedback control [75] to account for such experimentally controlled human data. While advances have been made, nobody would deny that this approach encounters challenges when the actions become more complex and realistic. This is particularly problematic when actions are no longer free, as in reaching, but involve contact with objects, ranging from pouring a glass of wine to moving the ribbon in gymnastics. Needless to say, current state-of-the-art movements of robots are still a far cry from those of Elena Kanaeva. Why do humans perform so much better, at least to date? What can robotic control learn from human neuromotor control?

1.1 *The Paradox: Delays and Noise in the Human Neuromotor System*

A first look into the biological neuromotor control system reveals some puzzling facts: information transmission in the human central nervous system is extremely slow and also very noisy. Action potentials, the basic unit of information coding, travel at a speed of approximately 100 m/s [32]; the shortest feedback loop is around 50 ms and reserved for startle reactions [35, 47]. When feedback is integral to more meaningful responses, loop times of 200 ms and longer are a more realistic estimate. In addition to such long delays, the biological neuromotor system displays noise and fluctuations at all levels [13]. The biological system is an extremely complex non-linear system with multiple levels of spatiotemporal scales, ranging from molecular and cellular processes to motor units and muscle contractions, and to overt behavior. Noise and fluctuations from all these levels manifest themselves at the behavioral level as ubiquitous variability. For example, in simple rhythmic finger tapping even trained musicians exhibit at least 5% variance of the period [19, 73]. In a discrete throwing action, humans display a limit in timing resolution of 9 ms [8]. Such large delays and high levels of noise pose extreme challenges for any control model. And yet, humans are amazingly agile and dexterous.

While the human controller appears clearly inferior to robotic systems, the biological “hardware” with its compliant muscles and soft tissues defy any comparison with the heavy actuators of robots. It seems highly likely that the dexterous human controller exploits these features. More recent developments in robotics have developed actuators with variable compliance, such as hands or grippers made of soft material [12] or actuators with mechanically adjustable series compliance [79]. However, the flexibility that comes with variable stiffness may also incur costs, such as loss in precision or higher energy demands. How do humans combine their software limitations and use their compliant and high-dimensional actuators to solve complex task demands?

1.2 *Intrinsic and Extrinsic Redundancy*

The biological sensorimotor system has a large number of hierarchical levels with high dimensionality on each level. One important consequence of this high dimensionality is that it affords redundancy and thereby an infinite variety of ways a given action is performed. At the behavioral level, hammering a nail into a wooden block can be achieved with multiple different arm trajectories and muscle activation patterns. The adage “repetitions without repetition” conveys that the ubiquitous and ever-present fluctuations prevent any action to be the same as another one. Importantly, this *intrinsic redundancy* faces an additional *extrinsic redundancy* that is inherent to the task. Imagine dart throwing: the bull’s eye or the rings on the dartboard allow a set of hits that achieve a given score. Further, orientation angle of the dart stuck

104 on the board does not change the score. Hence, tasks have extrinsic redundancy that
105 permits a *manifold of solutions* [69]. However, not all solutions are equally suitable:
106 some may not be biomechanically optimal, others may be risky, yet others may have
107 a lot of tolerance to error and noise. Examining human performance may reveal how
108 humans navigate the task's redundancy and preferences may give insight into the
109 controller. Hence, a suitably constructed extrinsic redundancy presents an important
110 entry point into examining human control, strategies, or objective functions.

111 ***1.3 An Agnostic Approach to Human Motor Control***

112 Recognizing these challenges, our research has adopted an approach with minimal
113 assumptions about human neuromotor control. Instead of starting with a hypothesized
114 controller and the plant, i.e., the brain and the musculo-skeletal system, connected
115 by forward and feedback loops transmitting motor and sensory signals, we take an
116 agnostic stance. We begin with what is known and can be analyzed: the physical task
117 that the actor performs. Under simplified conditions, very few assumptions need to
118 be made about the human controller.

119 This chapter will review this task-dynamic approach as it was developed in three
120 experimental paradigms that examine human interactive skills. These three skills
121 progress from the simple action of throwing a ball, to rhythmic intermittent bouncing
122 of a ball, to the continuous manipulation of a complex object, a cup with a rolling
123 ball inside, mimicking a cup of coffee – or a glass of wine. Mathematical analyses
124 and exemplary results will show that variability, stability and predictability matters
125 in human motor control. I will close with a still largely speculative hypothesis on
126 how the human control system generates such actions, a perspective that may be less
127 hampered by long delays and noise: control via dynamic primitives.

128 **2 A Task-Dynamic Approach to Understanding** 129 **Control of Interactions**

130 Using mathematical modeling and virtual technology we developed a task-dynamic
131 approach to study the acquisition and control of simple and more complex interactive
132 skills. Following a brief outline of the methodological steps, three exemplary lines
133 of research will be reviewed with some selected results.

134 2.1 Identifying a Motor Task

135 The important initial step is choosing a motor task that satisfies several desiderata:
136 First, it should represent a core aspect germane to many other tasks that is “inter-
137 esting” from a control perspective. Second, the motor task should have redundancy:
138 the well-defined goal should allow for a variety of solutions to achieve the task goal.
139 Third, the task should be novel and sufficiently challenging to require practice to
140 achieve success. The changes over practice provide an important lens to reveal how
141 humans navigate through the space of solutions. (Note this differs from studying
142 everyday behaviors, such as reaching or grasping, where only adaptations to novel
143 scenarios produce change.) Fourth, improvement should happen within one or few
144 experimental session(s), but should also allow for fine-tuning over a longer time
145 scale. These stages are likely to reveal processes underlying motor learning.

146 We selected and designed three tasks: The arguably simplest (inter-)active task
147 is to throw a ball to a target. While the ball only needs to be released, the size and
148 location of the target imposes constraints on the release that fully determine the
149 projectile’s trajectory and thereby the hitting accuracy. A next step in interaction is
150 to repeatedly contact the ball – such as in bouncing a ball rhythmically in the air.
151 This intermittent interaction extends the control demands, as the propelled object
152 needs to be intercepted again. Any error at one contact influences the subsequent
153 contact – these repeated interactions render the task a dynamic system. The third task
154 takes interactions one significant step further: motivated by the seemingly mundane
155 action of carrying a cup of coffee, we designed a simplified task that exemplifies the
156 continuous interaction with a complex object.

157 2.2 Mathematical Model of the Task

158 Once the core control challenge is identified, the task is modeled mathematically to
159 formalize and prune away irrelevant aspects of the real-life task. A simple physical
160 model also facilitates subsequent analyses of both model and human data. What
161 system captures the essential demands of ball release and permits a full analysis of
162 the solution space? What is the simplest intermittent dynamical system that lends
163 itself to mathematical analysis? What is the simplest physical system that captures the
164 continuous interaction between the human and a dynamically complex object? One
165 core element in our mathematical modeling and analysis is the distinction between the
166 execution variables \mathbf{x} and the result variables \mathbf{r} : The result variable(s) are defined by
167 the task goal and the instruction to the subject and quantify the quality of performance.
168 This is typically an error measure, although this error measure can take many forms.
169 Execution variables are under control of the performer and determine the task result.
170 For the analysis it is important to identify all execution variables that fully determine
171 the result, in order to have an analytic or numerical understanding of the space of

172 solutions. The functional relation between execution and result is the essence of the
173 model and analysis: $\mathbf{r} = f(\mathbf{x})$.

174 **2.3 *Mathematical Analysis and Derivation of Hypotheses***

175 Based on the physical model, the space of all possible solutions to the task can be
176 derived. As the model system is typically nonlinear, the space of solutions may be
177 complex and solutions have additional properties, such as dynamic stability, risk, or
178 predictability, as elaborated below. The model structure determines the mathematical
179 tools that can be used to derive predictions. Core to our task-dynamic approach are
180 analyses of stability, error sensitivity, or robustness to perturbations and noise. Im-
181 portantly, exact quantitative hypotheses can be formulated that define those solutions
182 with the greatest probability of success.

183 **2.4 *Implementation in a Virtual Environment***

184 Based on the explicit mathematical model, the task is rendered in a virtual envi-
185 ronment that permits precise measurement of human execution and errors, i.e., the
186 execution and result variables. The execution variables are those that the subject con-
187 trols via interfacing with the virtual system. For example, while the subject performs
188 a throwing task, the real arm trajectory controls the ball release, but the ball and the
189 target are virtual. The virtual rendering has the advantage that it confines the task to
190 exactly the model variables and its known parameters. There are no uncontrolled as-
191 pects as would occur in a real experiment. Further, the parameters and result variables
192 can be freely manipulated to test hypotheses about human control strategies.

193 **2.5 *Measurement, Analysis, and Hypothesis Testing*** 194 ***of Human Performance***

195 Subjects interact with the virtual physics of the task via manipulanda that simul-
196 taneously render the task dynamics and measure human performance strategies.
197 The measured execution variables and the task result are then evaluated against the
198 mathematical analysis of the solution space. The virtual environment affords easy
199 manipulation of the model, its parameters, and specific task goals. Hypotheses about
200 preferred solutions are derived from model analysis and can be evaluated based on
201 the human data. As shown below, the task can be parameterized to create interesting
202 task variations to contrast alternative control hypotheses.

2.6 Interventions

Based on the findings, the controlled virtual environment can also be used to create interventions that guide or shape behavior. This is significant for clinical applications, where scientifically-grounded quantitative assessments and interventions are still rare. While this review will focus on the basic science issues, some applications to questions on motor control in children with dystonia or on interventions for the elderly can be found in Sternad [61], Chu et al. [5], Hasson and Sternad [24].

3 Throwing a Ball to Hit a Skittle – Variability, Noise, and Error-Tolerance

3.1 The Motor Task

This experimental paradigm was motivated by a ball game found in many pubs and playgrounds around the world: The actor throws a ball that is tethered to a virtual post by a string like a pendulum; the goal is to hit a target skittle (or skittles) on the opposite side of the pole (Fig. 1a). Accurate throwing requires a controlled hand/ball trajectory that prepares the ball release at exactly the right position with the right velocity to send the ball onto a trajectory that knocks over the target skittle. The practical advantage of this game is that the tethered ball cannot be lost and the game can be played in a small space; the theoretical advantage is that the pendular motions of the ball introduce “interesting” dynamics with a nonlinear solution space including discontinuities that present challenges to trivial learning strategies such as gradient descent. Importantly, the task has redundancy and thereby offers a manifold of solutions with different properties.

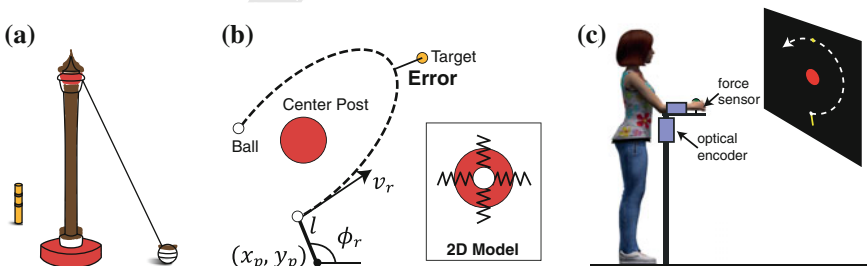


Fig. 1 The virtual throwing task. **a** Schematic of the real task. **b** The 2D model from a top-down view. **c** The experimental set-up with force and position sensors for recording of human movement. Measured movements are shown in real time on the screen (Reproduced from [69])

3.2 The Model and Its Virtual Implementation

To simplify the three-dimensional task, the ball was confined to the horizontal plane, eliminating the pendular elevation during excursion (Fig. 1b). In the model, the ball is attached to two orthogonal, massless springs with its rest position at the center post. In the virtual implementation, the actor views the workspace from above on a backprojection screen (Fig. 1c). S/he throws the virtual ball by moving his/her real arm in a manipulandum that measures the forearm rotations with an optical encoder; these measured movements are shown online by a virtual lever arm (Fig. 1b). Deflecting the ball from the rest position and throwing the ball with a given release angle and velocity, the ball traverses an elliptic path generated by the restoring forces of the two springs. The following equations describe the ball motion in the $x - y$ coordinates of the workspace:

$$\begin{pmatrix} x(t) \\ y(t) \end{pmatrix} = \begin{pmatrix} x_p \\ y_p \end{pmatrix} \cos \omega t + \begin{pmatrix} \cos \phi_r & -\sin \phi_r \\ -\sin \phi_r & \cos \phi_r \end{pmatrix} \begin{pmatrix} l \cos \omega t \\ v_r / \omega t \end{pmatrix} \quad (1)$$

ω denotes the natural frequency of the springs, (x_p, y_p) denotes the lever's pivot point, and l the length of the arm (Fig. 1b). Damping of the springs can be added; asymmetric damping and also stiffness may be used to introduce a more complex force field in the workspace. For a given throw, the two execution variables angle ϕ_r and velocity v_r of the virtual hand at ball release fully determine the ball trajectory in the workspace $x(t), y(t)$ (for more details see [7]).

The actor's goal is to throw the ball to hit the target skittle, without hitting the center post. The latter restriction eliminates simple ball releases with zero velocity. Post hits are therefore penalized with a large fixed error. Otherwise, error is defined as the minimum distance between the ball trajectory and the target center (Fig. 1b). Thus, the result variable is the scalar error that is fully determined by ϕ_r and v_r . Importantly, there is more than one combination of ϕ_r and v_r that leads to zero error, i.e. the task has the simplest kind of redundancy: two variables map onto one. While this low dimensionality permits easy visualization in 3D to develop intuitions, the solution manifold for zero-error solutions can also be analytically derived and expressed in implicit form:

$$\frac{v_r}{\omega} = \frac{|(-l \sin \phi_r - y_p) x_t + (l \cos \phi_r + x_p) y_t|}{\sqrt{(l + \cos \phi_r x_p + \sin \phi_r y_p)^2 - (\cos \phi_r x_t + \sin \phi_r y_t)^2}} \quad (2)$$

3.3 Geometry of the Solution Space

Figure 2 illustrates two different target constellations that generate two different topologies of the result space [62]. Figure 2a, b show the top-down view of the

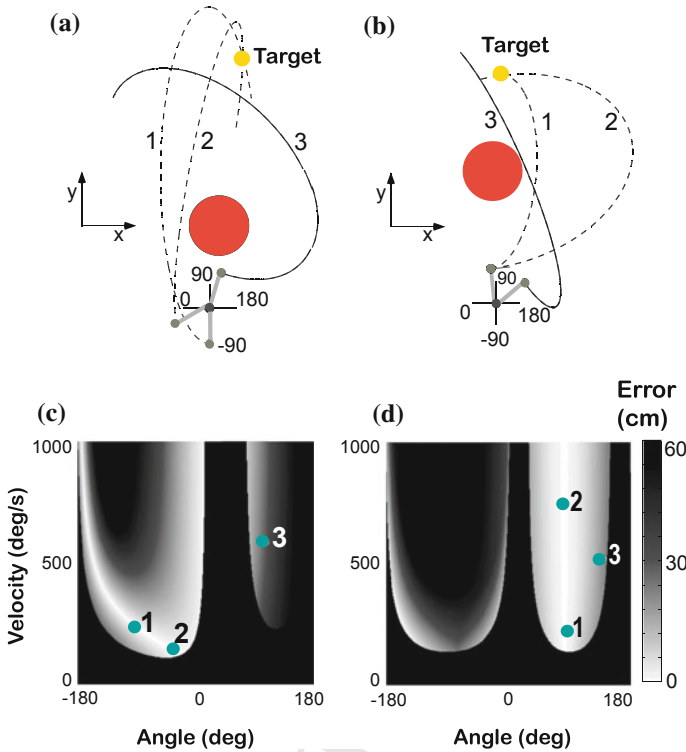


Fig. 2 Two target constellations (a, b) and their corresponding result spaces (c, d). For each task, three exemplary ball trajectories are shown which correspond to the three release points plotted in the result spaces (*green dots*). *White* denotes zero-error solutions, increasing error is shown by increasingly *darker grey shades*, *black* denotes a post hit. In both constellations, two ball trajectories exemplify how different release variables can lead to the same result with zero error (1, 2, *dashed lines*). Trajectory 3 shows a trajectory that does not intersect the target (Modified from [62])

258 workspace with the red circle representing the center post and the yellow circle the
 259 target. The manipulandum is shown at the bottom with its angular coordinates. The
 260 three elliptic trajectories are three exemplary ball trajectories with different release
 261 angles and velocities. In both work spaces two ball trajectories (1, 2) go through the
 262 target and have zero error, while one (3) has a non-zero error. Figure 2c, d show
 263 the respective result spaces, spanned by release angle and velocity; error is depicted
 264 by shades of gray, with lighter shades indicating smaller errors. *White* denotes the
 265 zero-error solutions, or the solution manifold. *Black* signifies those releases that hit
 266 the center post, which incur a penalty in the experiment. The three points are the ball
 267 releases pertaining to the three ball trajectories above.

268 The two result spaces present several interesting features: In target constellation
 269 A the solution manifold has a nonlinear J-shape that represents solutions over a
 270 wide range of release velocities and angles. As indicated by the grey shades, the

271 regions adjacent to the solution manifold have different gradients and the sensitivity
272 of the zero-error solution changes along the solution manifold. Further, the region
273 on the J-shaped manifold with the lowest sensitivity is directly adjacent to the black
274 penalty region. Hence, strategies with the lowest velocity were adjacent to penalized
275 post hits; this poses risk and a simple gradient descent may run into problems. In
276 target constellation B the zero-error solutions are independent of velocity and fully
277 specified by the release angle, as the solution manifold runs parallel to velocity. As
278 visible from color shading, low-velocity solutions have slightly less error tolerance
279 compared to high-velocity solutions and again transition directly into the penalty
280 region. Note that other target locations have yet different geometries of the solution
281 manifold creating different challenges to the performer [69].

282 3.4 Generating Hypotheses from Task Analysis

283 One study created two result spaces with different topologies to generate specific
284 predictions [62]. Given that humans have limited control accuracy due to the per-
285 vasive noise in their neuromotor system, we hypothesized that in such redundant
286 tasks humans seek solutions that are tolerant to their intrinsic noise and also to
287 extrinsic perturbations (*Hypothesis 1*). Such error-tolerant solutions have higher like-
288 lihood to be accurate and would therefore also obviate some error corrections. This
289 is advantageous as error corrections incur computational cost and, importantly, the
290 sensorimotor feedback loop suffers from the long delays in the human system. Note
291 that our definition of error tolerance differs from standard sensitivity analyses that
292 assess local sensitivity in a linearized neighborhood. As humans make relatively
293 large errors and the topology is highly nonlinear, we calculated error tolerance as the
294 average error over an extended neighborhood around a chosen solution; this neigh-
295 borhood is defined by the individual's variability. An alternative hypothesis was that
296 humans select strategies that minimize velocity at release to avoid costs associated
297 with higher effort or signal-dependent noise (*Hypothesis 2*). There is much evidence
298 that movements at slow velocity are preferred, as higher speed tends to decrease
299 accuracy (speed-accuracy trade-off) [16, 17, 42]. This observation concurs with the
300 information-theoretical expectation that noise increases with signal strength. In mo-
301 tor control, signal strength is typically equated with firing rate of action potentials,
302 i.e. force magnitude or, in the dynamic case, movement velocity. A third hypothesis
303 discussed in the human motor control literature is that risk is avoided, and participants
304 stay at a distance from the penalty area (*Hypothesis 3*) [6, 40, 48].

305 3.5 Error Tolerance Over Minimizing Velocity and Risk

306 Nine participants practiced 540 and 900 throws with Task A and B, respectively.
307 Figure 3 illustrate the predictions as computed for *Hypothesis 1* and 2 in the top

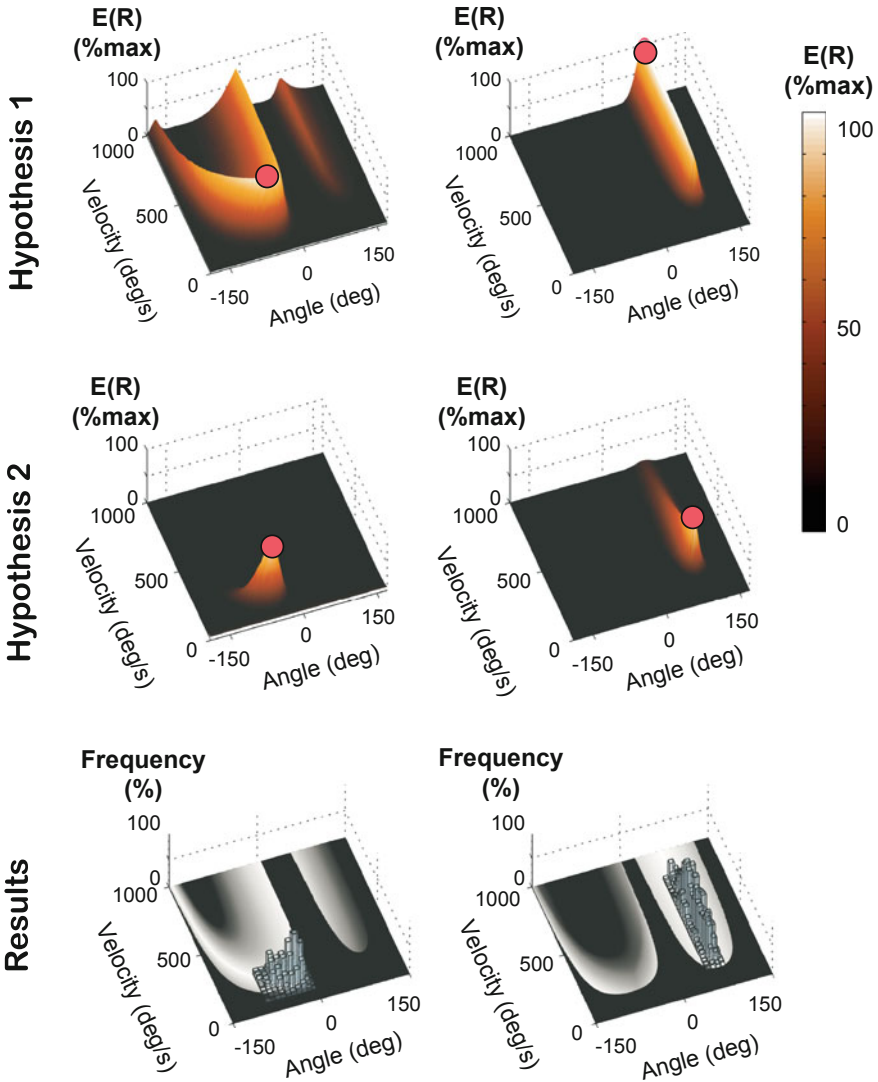


Fig. 3 Hypotheses and experimental results for two task **a** (left column) and task **b** (right column). The *top* row shows the expected results, $E(R)$ for *Hypothesis 1*: Maximizing error tolerance; the *second* row shows simulated predictions for *Hypothesis 2*: Minimizing velocity and signal-dependent noise. The expected result $E(R)$ was computed as average error over a neighborhood scaled by a softmax function (for details see [62]). The peaks highlighted by the *red circles* denote the expected solutions. The *third* row shows the data as histograms plotted over the result spaces to compare against the predicted solutions (Modified from [62])

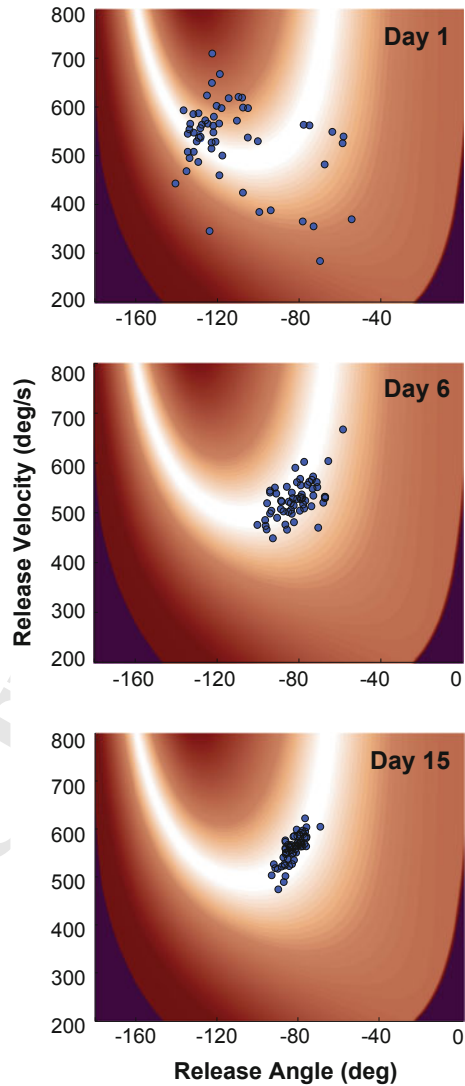
308 two rows. Error tolerance was quantified as the expected error over a neighborhood
309 around each strategy, simulating that human strategies are noisy, scaled by a softmax
310 function, $E(R)$. For *Hypothesis 2*, expected velocity was computed over the same
311 neighborhood, again scaled by a softmax function. The solutions that are most error-
312 tolerant and those with lowest velocity are indicated by red circles in the middle
313 panels. Examining all throws after removing the initial transients, the bottom panels
314 show the histograms of all subjects' releases in both result spaces (from Fig. 2c, d).
315 In Task A the data distribution clustered along the solution manifold at low velocities
316 and close to the discontinuity. The mode at angle 236° and velocity 136 deg/s was
317 close to the maximally error-tolerant point as predicted by *Hypothesis 1*. However,
318 the solutions also had relatively low velocity, which was consistent with *Hypothesis*
319 *2*. These two benefits seemed to outweigh that these solutions were close to the high-
320 penalty area, i.e. risky strategies were not avoided, counter to *Hypothesis 3*. Task B
321 was designed to dissociate *Hypotheses 1* and *2*. The histograms on the right panel
322 illustrate that the data were distributed across a large range of velocities between
323 140 and 880 deg/s, with the mode of the data distribution at 544 deg/s, although
324 individual preferences were more clustered on the velocity axes. The fact that indi-
325 viduals chose solutions over a wide range of velocities, without a specific preference
326 for low-velocity or the high-tolerance point was at first sight inconsistent with both
327 *Hypothesis 1* and *2*. However, in further analysis the observed variability of each
328 individual was regressed against release velocity and revealed that variability did not
329 increase at higher velocities, as would be expected from *Hypothesis 2*. Instead, these
330 analyses showed that strategies were better explained by error-tolerance, consistent
331 with *Hypothesis 1* (for details see [62]).

332 Taken together, this first study showed how a task analysis can generate predictions
333 that permit direct tests based on human data. The conclusion from this study is that
334 humans seek out error-tolerant strategies, i.e., those where variability at the execution
335 level has minimal detrimental effect on the result. As these strategies attenuate noise
336 effects on the result, fewer errors occur that in turn require fewer corrections to stay
337 on target. This not only reduces computations but also diminishes the negative effect
338 that delays may cause.

339 3.6 Tolerance, Covariation, and Noise

340 Increasing error-tolerance is only one of three avenues to deal with unavoidable
341 variability in execution. Two more, conceptually different avenues exist for how
342 variability can be transformed to lessen its effect on the task result. Figure 4 illustrates
343 this notion with data from a representative subject who practiced the same throwing
344 task for 15 days, 240 throws per day [7]. The geometry of the result space shows a U-
345 shaped solution manifold due to a different target constellation. The broad scatter of
346 the data on Day 1 reflects initial exploratory attempts with inferior results compared
347 to those after some practice. Most visibly, on Day 6 the data not only *translated* to a
348 location on the solution manifold with more error-tolerance (shown as a wider band

Fig. 4 Data from an exemplary subject who practiced the throwing task for 15 days. The initially broad scatter translated to a more error-tolerant strategy, rotated to covary with the solution manifold (*white*) and scaled of reduced the amplitude of dispersion over the course of practice (Modified from Cohen and Sternad [7])



349 of white), but the observed variability also started to *covary* with the direction of
 350 the solution manifold, while overall variability was only moderately reduced. The
 351 distribution on Day 15 clearly reveals a third transformation: the overall dispersion
 352 was significantly reduced or *scaled*, over and above the further enhanced covariation.
 353 These three data transformations, corresponding to the matrix transformations of
 354 translation, rotation, and scaling, were numerically quantified from individual data
 355 distributions as costs: The average result of a given data set could be improved by
 356 1.2 cm on Day 1, if it were translated to the optimal location. The difference in average

357 result from actual to optimal renders *Tolerance-cost*. If the actual data were rotated
 358 or permuted optimally, the difference in result with the real data would quantify
 359 *Covariation-cost*. If the real data distribution was scaled or its noise was reduced
 360 optimally, the difference between initial and optimal data quantifies *Noise-cost*. The
 361 parallel but differential evolution of the three costs was shown in Cohen and Sternad
 362 [7].

363 3.7 Covariation, Sensitivity to Geometry of Result Space 364 in Trial-by-Trial Learning

365 A separate study specifically focused on covariation and examined not only the
 366 distributions of the data, but also their temporal evolution to assess whether subjects'
 367 trial-by-trial updates were sensitive to the direction of the solution manifold [1]. Three
 368 detailed hypotheses guided our experimental evaluation: *Hypothesis 1*: Humans are
 369 sensitive to the direction of the solution manifold reflected in preferred directions
 370 of their trial-to-trial updates. *Hypothesis 2*: This direction-sensitivity becomes more
 371 pronounced with practice. *Hypothesis 3*: The distributional and temporal structure
 372 is oriented in directions orthogonal and parallel to the solution manifold. Note that
 373 sensitivity to the directions of the null space is also core to several other approaches,
 374 which employ covariance-based analyses that linearize around the point of interest
 375 using standard null space analysis [10, 55]. In contrast to our approach, those analyses
 376 do not exploit the entire nonlinear geometry of the result space.

377 Thirteen subjects practiced for 6 days throwing to the same target as above, with
 378 240 throws per day (4 blocks of 60 trials). To assess the distribution and also trial-
 379 to-trial evolution, each block of 60 throws was examined as illustrated in Fig. 5a.
 380 To assess whether the trial-to-trial changes had a directional preference, the 60 data
 381 points were projected onto lines through the center of the data set (red lines in Fig. 5a).
 382 The center was typically on or was close to the solution manifold. The direction
 383 parallel to the solution manifold was defined as θ_{par} , the direction orthogonal to the
 384 solution manifold was defined as θ_{ort} . The time series of the projected data was then
 385 analyzed using autocorrelation and Detrended Fluctuation Analysis (DFA).

386 This line was then rotated through $0 < \theta < \pi$ rad, in 100 steps, with its pivot
 387 at the center of the data. At each rotation angle θ , the data were projected onto the
 388 line and time series analyses conducted. We expected that in directions orthogonal
 389 to the solution manifold θ_{ort} successive trials show negative lag-1 autocorrelation,
 390 reflecting error corrections; in the parallel direction θ_{par} correction was not necessary,
 391 as deviations have no effect on the task result. Note that the result space is spanned
 392 by angle and velocity, i.e. with different units; hence, both axes had to be normalized
 393 to each individual's variance to ensure orthogonality and a metric.

394 Figure 5b shows two time series of projected data from those directions that
 395 rendered maximum and minimum anti-correlation. Note the visible difference in
 396 temporal structure, reflecting that direction in the result space does matter. Plotting

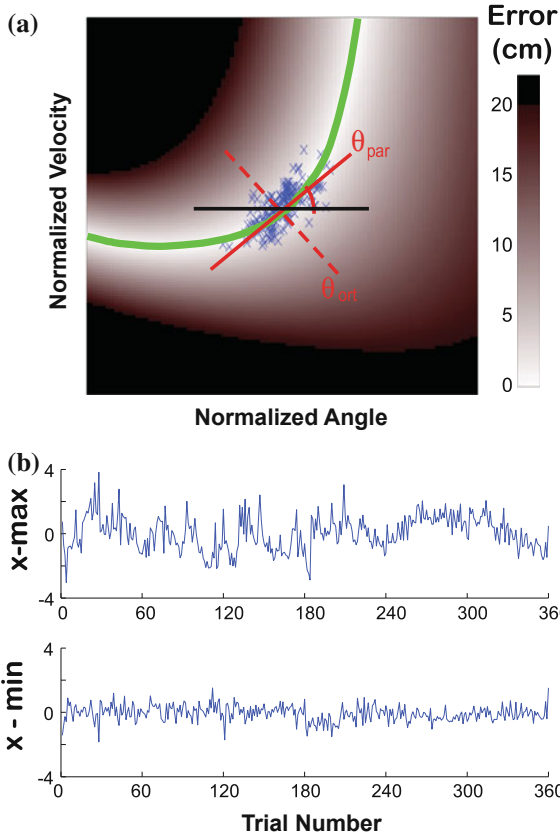


Fig. 5 **a** Result space with solution manifold (*green*), with angle and velocity normalized to variability of each individual. *Red lines* denote directions parallel and orthogonal to the solution manifold. The *black line* denotes $= 0$ rad. Data are projected onto lines between $0 < \theta < \pi$ rad and autocorrelations are computed for each projection. **b** Time series of projected data where autocorrelation was at a minimum and a maximum. Note that these directions do not necessarily correspond to parallel and orthogonal directions (Reproduced from [1])

397 the results of the lag-1 autocorrelations across angle of the projection in Fig. 6 reveals
 398 a marked modulation: The red lines (with variance across subjects) show autocorrelation
 399 values for each rotation angle. The modulation supports *Hypothesis 1* that
 400 trial-by-trial updates are sensitive to the angle, and implicitly, the direction of the
 401 solution manifold. The green vertical lines denote the direction of the solution manifold.
 402 The minima and maxima of the autocorrelation values are indicated by triangles.
 403 Consistent with *Hypothesis 2*, the modulation gets more pronounced across the three
 404 practice blocks, expressing that after the initial stage, trial-to-trial dynamics became
 405 more directionally sensitive. The structure in the orthogonal direction changed from
 406 initially positive autocorrelations to white noise and eventually very small negative
 407 values [1].

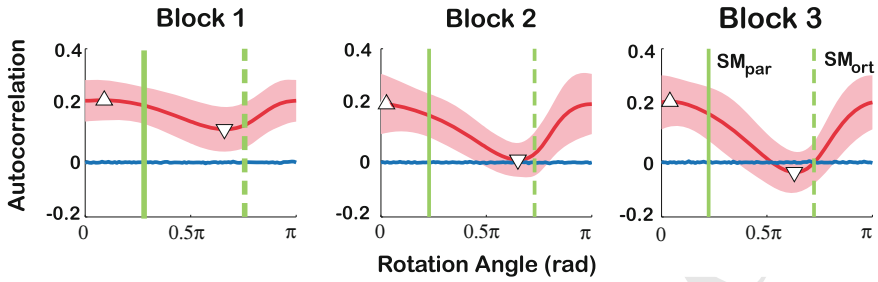


Fig. 6 Autocorrelation of time series of projected data in all directions in result space. The modulation across directions becomes more pronounced with practice, expressing increased sensitivity to the geometry of the result space. Note that while the extrema are close to the directions of the solution manifold (SM_{par} and SM_{ort}) they are not coincident (Modified from [1])

3.8 Orthogonality and Sensitivity to Coordinates

This analysis also revealed important discrepancies to *Hypothesis 3*. The directions of minimum and maximum autocorrelation were near, but not coincident with the orthogonal and parallel directions, as hypothesized. This finding alerts to an important issue: orthogonality is sensitively dependent on the chosen variables. In the present case, the original physical variables, angle and velocity, had different units and required normalization. While technically correct, it raises the question whether these units accurately reflect the units of the central nervous system. One important caveat for this and related approaches is that the structure of variability is fundamentally sensitive to the chosen coordinates.

This fact was highlighted in a separate study, which showed that this sensitivity is particularly pertinent for covariance-based analyses [70]. Even simple linear transformations can critically alter the results, as demonstrated by a simulation that analyzed variability in joint space: for two different definitions of joint angles, anisotropy of a data distribution can change. While covariance-based analysis of anisotropy of data is dependent on the coordinates, we demonstrated that our analysis of error tolerance, covariation and noise is significantly less sensitive, as it projects the execution variables into the result space. Nevertheless, these critical questions open an interesting avenue for conceptually deeper questions: What are the coordinates of the nervous system? What is the appropriate metric? What is the best or most suitable representation of the problem? While data may be dependent on the coordinates, can data be used to reversely shed light on the coordinates that the nervous system uses?

To pursue these questions, the study by Abe and Sternad further examined how a rescaling of the execution variables in a simple model of task performance with similar redundancy may reproduce these deviations [1]. While this revealed possible sources for these observations, much more work is needed. For example, scaled noise in different execution variables or sensory signals might also give rise to such “deviations”. These are clearly important issues for understanding biological

436 movement control, and possibly also worth reflection when designing control in
437 robotic systems.

438 **3.9 Interim Summary**

439 The throwing skill illustrated our model-based approach and its opportunities to
440 shed light on human control. The findings showed that humans choose strategies that
441 obviate the potentially detrimental effects of intrinsic noise. With less noise and
442 variability, less error corrections are needed. Error corrections are not only compu-
443 tationally costly, they are also hampered by the slow transmission speed in biologi-
444 cal systems. Are similar strategies also possible in different tasks, especially when
445 interacting with an object?

446 **4 Rhythmic Bouncing of a Ball – Dynamic Stability** 447 **in Intermittent Interactions**

448 **4.1 The Motor Task**

449 Rhythmically bouncing a ball on a racket is a playful and seemingly simple task. Yet,
450 it requires a high degree of visually-guided coordination to intercept the ball at the
451 right position and with the right velocity to reach a target amplitude and perform in
452 a rhythmic fashion (Fig. 7a–c). As in the throwing task, success is determined at one
453 critical moment when the racket intercepts the ball, as this impact fully determines
454 its amplitude. Hence, the core challenge of this task is the control of collisions, a
455 feature germane to numerous other behaviors, ranging from controlling foot-ground
456 impact in running to playing the drums. One key difference to throwing is that these
457 impacts are performed in a repeated fashion, and errors from one contact propagate
458 to the next. Hence, the actor becomes part of a hybrid dynamical system combining
459 discrete and continuous dynamics [11, 44, 46, 53].

460 **4.2 The Model**

461 The physical model for this task is again an extremely simple dynamical system,
462 originally developed for a particle bouncing on a vibrating surface [21, 76]. The
463 model consists of a planar surface moving sinusoidally in the vertical direction; a
464 point mass moving in the gravitational field impacts the surface with instantaneous
465 contact (Fig. 7b). The vertical position of the ball x_b between the k th and the $k + 1$ th
466 racket-ball impact follows ballistic flight:

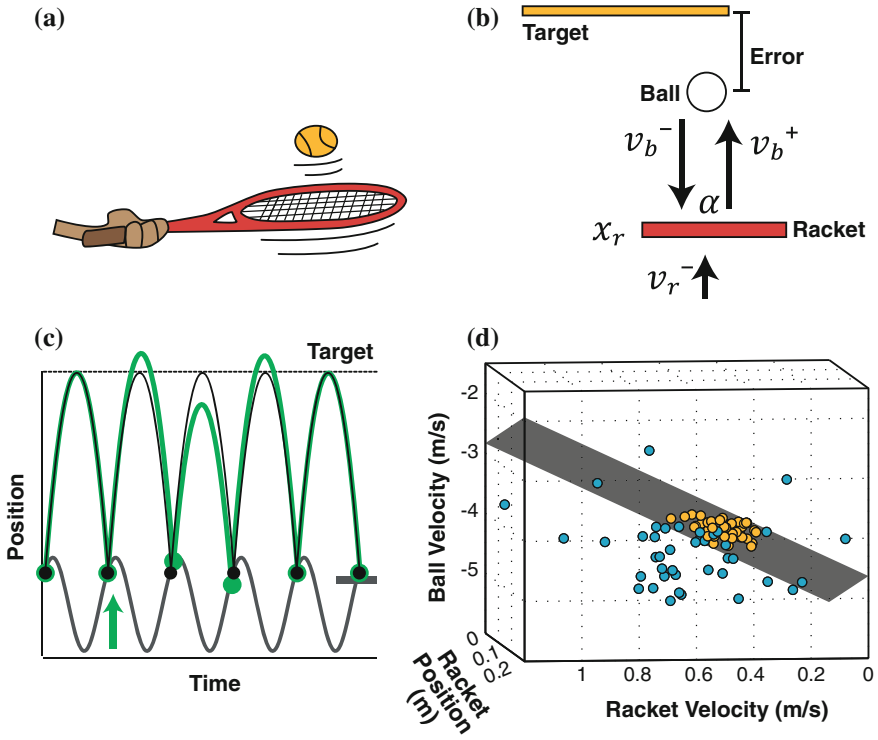


Fig. 7 Bouncing a ball with a racket. **a** The real task. **b** The physical and mathematical model. **c** Simulated time series assuming invariant sine waves of the racket. **d** Redundancy of the result space: Racket position and velocity and ball velocity determine ball amplitude. *Blue* data points are from early practice, *yellow* data points are from late practice (Reproduced from [69])

$$x_b(t) = x_r(t_k) + v_b^+(t - t_k) - g/2(t - t_k)^2$$

467 where x_r is racket position, v_b^+ is the ball velocity just after impact, t_k is the time of the
 468 k th ball-racket impact, and g is the acceleration due to gravity. With the assumption
 469 of instantaneous impact, the ball velocity just after impact v_b^+ is determined by:

$$v_b^+ = ((1 + \alpha)v_r^- - \alpha v_b^-)$$

470 where v_b^- and v_r^- are the ball and racket velocities just before impact, and the energy
 471 loss at the collision is expressed in the coefficient of restitution α . The maximum
 472 height of the ball between t_k and t_{k+1} depends on v_b^- and v_r^- and the position at impact
 473 x_r :

$$474 \max_{t_k \leq t \leq t_{k+1}} x_b(t) = x_r(t_k) + (((1 + \alpha)v_r^- - \alpha v_b^-)(t - t_k))^2 / 2g \quad (3)$$

4.3 Redundancy

The task goal is to bounce the ball to a target height, and the error is defined as the deviation from the maximum height (Fig. 7c). Even in this simplified form, the task has redundancy, as the result variable error is determined by three execution variables: v_b^- , v_r^- and x_r . Figure 7d shows the execution space with the solution manifold, i.e. the planar surface that represents all solutions leading to zero error. The blue and yellow data points are two exemplary data sets from early and late practice, respectively; each data point corresponds to one ball-racket contact. As to be expected, the early (blue) data show a lot of scatter, while the late practice data (yellow) cluster around the solution manifold.

4.4 Dynamic Stability

While the redundancy analysis is performed on separate collisions, the racket and ball model also lends itself to dynamic stability analysis. To facilitate analysis, the racket movements are assumed to be sinusoidal, such that racket position and velocity at impact collapse into a single state variable, racket phase θ_k . Applying a Poincare section at the ball-racket contact, where x_r and x_b are identical, a discrete map can be derived with v_k^+ and θ_k as state variables:

$$\begin{aligned} v_{k+1}^+ &= (1 + \alpha)A\omega \cos \theta_{k+1} - \alpha v_k^+ + g\alpha(\theta_{k+1} - \theta_k)/\omega \\ 0 &= A\omega^2(\sin \theta_k - \sin \theta_{k+1}) + v_k^+ \omega(\theta_{k+1} - \theta_k) - g/2(\theta_{k+1} - \theta_k)^2 \end{aligned} \quad (4)$$

A and ω are the amplitude and frequency of the sinusoidal racket movements [11, 53, 66]. This nonlinear system displays dynamic stability and, despite its simplicity, shows the complex dynamics of a period-doubling route to chaos [21, 76]. For present purposes, only stable fixed-point solutions are considered as they correspond to rhythmic bouncing. Local linear stability analysis of this discrete map identifies a stable fixed point, if racket acceleration at impact a_r satisfies the inequality:

$$-2g \frac{(1 + \alpha^2)}{(1 + \alpha)^2} < a_r < 0 \quad (5)$$

4.5 Hypotheses

In this dynamically stable state, small perturbations of the racket or ball die out without requiring corrections. Hence, if subjects establish such dynamically stable regime, they need not correct for small perturbations that may arise from the persistent neuromotor noise. Thus, we hypothesized that subjects learn these “smart” solution and exploit dynamic stability by hitting the ball with negative racket accel-

506 ation (*Hypothesis 1*). Further, due to the system's redundancy infinitely many stable
 507 solutions can be adopted. Hence, we administered perturbations to test if subjects
 508 established and re-established such stable states (*Hypothesis 2*).

509 **4.6 Virtual Implementation**

510 In the experiments, the participant stood in front of a projection screen and rhythmically
 511 bounced the virtual ball to a target line using a real table tennis racket. Similar
 512 to the throwing task, the projected racket movements were shown on the screen in
 513 real time impacting the ball. The display was minimal and only showed the modeled
 514 and measured elements, a horizontal racket and a ball both moving vertically to a
 515 target height (Fig. 7b). A light rigid rod was attached to the racket and ran through
 516 a wheel, whose rotations were registered by an optical encoder, which measured
 517 the vertical displacement of the racket, in analogy with the model, and shown on
 518 the screen. Racket velocity was continuously calculated. The vertical position of the
 519 virtual ball was calculated using the ballistic flight equation initialized with values at
 520 contact. To simulate the haptic sensation of a real ball-racket contact, a mechanical
 521 brake, attached to the rod, was activated at each bounce and decelerated the up-
 522 ward motions. Racket acceleration at or just before the impact was analyzed after the
 523 experiment and served as the primary measure of dynamic stability to test
 524 *Hypothesis 1* [80]. Ball position and velocity and racket velocity at contact were
 525 measured and analyzed to evaluate the data with respect to the solution manifold
 526 (*Hypothesis 2*).

527 **4.7 Learning and Adaptation to Perturbations**

528 Did human subjects seek and exploit dynamic stability of the racket-ball system?
 529 How robust is this system if the actor has to change and adapt to new situations? An
 530 experiment tested these questions in two stages: On Day 1, 8 subjects performed a
 531 sequence of 48 trials of rhythmic bouncing to a target height, each trial lasting 60 s.
 532 With the target height at 0.8 m from lowest racket position, and $\alpha = 0.6$, the average
 533 period between repeated contacts was 0.6 s, leading to approximately 100 contacts
 534 per trial. On Day 2, subjects performed 10 trials under the same conditions as on
 535 Day 1, but then performed another 48 trials after a perturbation was implemented.

536 *Stage 1:* Figure 8a shows the ball amplitude errors averaged of all subjects across
 537 48 trials. As expected, the error decreased with practice with a close-to exponential
 538 decline. Concomitantly, the acceleration of the racket at contact decreased from an
 539 initially positive to a negative value, indicative of performance attaining dynamic
 540 stability (Fig. 8b). Importantly, it took approximately 11 trials for subjects to “dis-
 541 cover” this strategy, showing that it was not trivial and required practice to learn it.
 542 The parallel evolution of both error and racket acceleration with practice provide
 543 strong support for *Hypothesis 1* that subjects seek dynamic stability.

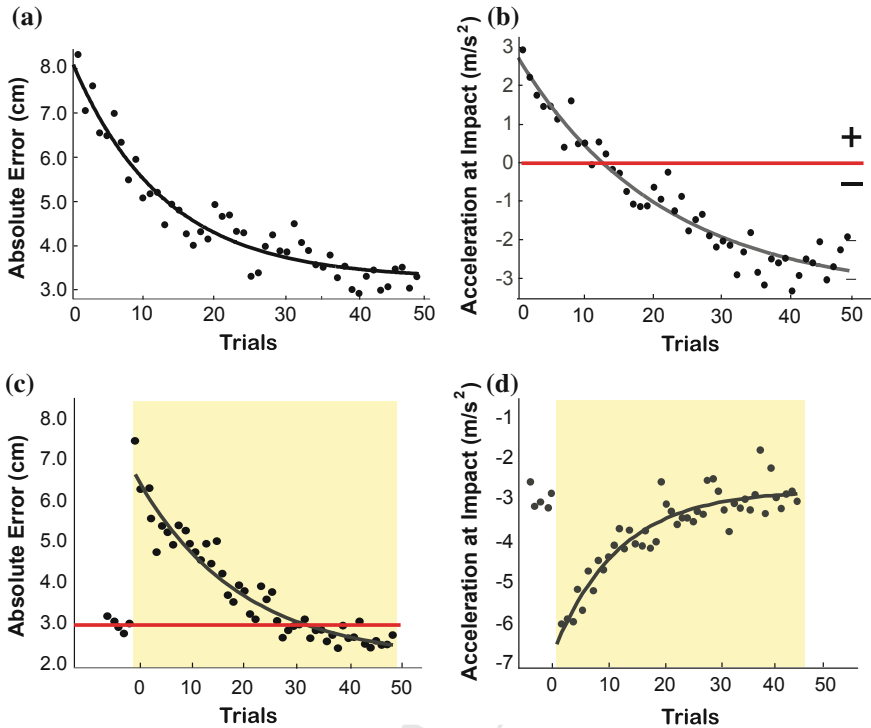


Fig. 8 Ball amplitude errors and racket accelerations over 48 trials. All data points are averages over 8 subjects. **a, b** Stage 1 of the experiment. **c, d** Stage 2 of the experiment. The shading denotes the perturbed trials

544 *Stage 2:* The second experimental session presented an even stronger test. Starting
 545 with 10 regular trials as on Day 1, subjects were exposed to a perturbation over the
 546 subsequent 48 trials (yellow shading in Fig. 8c, d). This perturbation was calculated
 547 using the redundancy of the execution: three execution variables, v_b^- , v_r^- and x_r ,
 548 determined the one result variable, absolute error of ball peak amplitude to the target
 549 height. Following Day 1, the average and standard deviations of v_b^- and v_r^- and
 550 x_r of the first 10 baseline trials were calculated for each individual to render an
 551 ellipsoid in result space representing the individually preferred solution (9). In the
 552 subsequent perturbed trials this preferred strategy was penalized with an error in ball
 553 amplitude. This error was delivered by replacing the veridical ball release velocity
 554 with one calculated based on the execution ellipsoid. This new ball velocity over-
 555 or undershot the target height as calculated. By simply replacing the ball velocity
 556 at the discontinuity, subjects did not explicitly perceive the perturbation. Within
 557 the ellipsoid, the penalty was maximal at its centroid and it linearly decreased to
 558 zero towards the boundaries (defined by one standard deviation around its centroid).
 559 Hence, assuming sensitivity to the gradient in result space and the redundancy of
 560 the task, subjects were expected to search for a new un-penalized solution. This

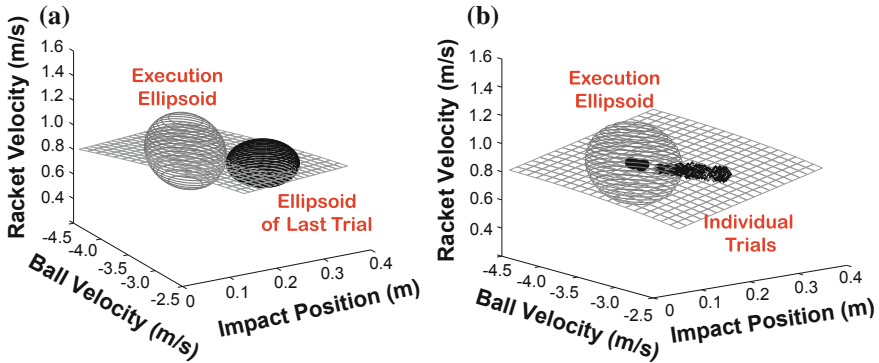


Fig. 9 Presentation of performance in execution space; the planar surface is the solution manifold. **a** The large execution ellipsoid represents the initially preferred strategy that is subsequently penalized during the perturbation phase. The smaller ellipsoid represents the final strategy that is established during the perturbation phase to avoid the penalty. **b** The right panel shows the same data and execution ellipsoid. The points are the sequence of trial means following the perturbation onset. It shows that subjects stay on the manifold but migrate outside the penalty ellipsoid

561 perturbation was calculated and delivered only in the virtual display such that subjects
 562 saw their drop in performance, but did not notice its cause explicitly.

563 Figure 9 illustrates the performance of one representative subject. Starting with the
 564 (larger) execution ellipsoid from the initial 10 trials (Fig. 9a), upon onset of the perturbation
 565 the subject gradually translated her execution along the planar solution manifold
 566 to a new location. The smaller and darker ellipsoid on the right depicts the average
 567 execution of the last trial: The strategy shifted and the variability decreased even
 568 further; importantly, there was no overlap with the initial ellipsoid (*Hypothesis 2*).
 569 This illustrates that the subject not only found a new successful solution without
 570 penalty, but the non-overlap also suggested that the subject was aware of her variability.
 571

572 Returning to the measures of error and racket acceleration at impact for these same
 573 data, shown in Fig. 8c, d, reveals that upon perturbation onset, both errors and racket
 574 acceleration changed significantly as expected. However, over the course of the 48
 575 perturbed trials, subjects incrementally decreased their errors and reestablished the
 576 previously preferred racket acceleration of -3 m/s^2 . In fact, this acceleration value
 577 was determined to be optimal for the given parameters in additional Lyapunov analyses
 578 of the model system [53]. This result shows that subjects successfully established
 579 dynamic stability in multiple different ways.

580 Experimental evidence that subjects learn to hit the ball with a decelerating racket
 581 has been replicated in several different scenarios. The different experimental set-ups
 582 included a pantograph linkage with precise control of the haptic contact, a real tennis
 583 racket to bounce a real ball attached to a boom, and freely bouncing a real ball in
 584 3D [66, 67]. The findings were robust: with experience performers learn to hit the
 585 ball with negative racket acceleration; based on stability analyses of the model we

586 concluded that they learn to tune into the dynamic stability of the racket-ball system.
587 Based on these findings, we also designed an intervention to guide subjects towards
588 this dynamically stable solution. Manipulating the contact parameters via a state-
589 based shift indeed successfully accelerated subjects' learning the dynamically stable
590 solution, which correlated with faster performance improvement [30].

591 **4.8 Interim Summary**

592 These studies provided strong evidence that humans seek dynamic stability in a
593 task, a solution that is computationally efficient as small errors and noise converge
594 without necessitating explicit error correction. In the face of perturbations, subjects
595 successfully navigated the result space and established new solutions available due to
596 the redundancy. There was also evidence that they were aware of their own variability.
597 As in skittles, subjects seek solutions where noise matters less.

598 **5 Chaos in a Coffee Cup – Predictability in Continuous** 599 **Object Control**

600 **5.1 The Motor Task**

601 Leading a cup of coffee to one's mouth to drink is a seemingly straightforward action.
602 However, transporting a cup filled with sloshing fluid to safely contact the mouth
603 without spilling remains a challenge not to be underestimated for both humans and
604 robots. Carrying a cup of coffee (or a glass of wine) exemplifies a class of tasks that
605 require continuous control of an object that has internal degrees of freedom. How
606 do humans control interactions with such an object, where the sloshing fluid creates
607 time-varying, state-dependent forces that have to be preempted and compensated to
608 avoid spill? Can humans or robots really have a sufficiently accurate internal model
609 of the complex fluid dynamics to online predict and react to the complex interaction
610 forces? In search of human strategies that apparently deal with this problem easily,
611 we started again with the analysis of the task dynamics, following the steps outlined
612 above.

613 **5.2 The Model**

614 In principle, the task presents a problem in fluid dynamics [38, 49]. To make this
615 complex infinitely-dimensional system more tractable, several simplifications were
616 made [23]: (1) the 3D cup was reduced to 2D, (2) the sloshing coffee was reduced to

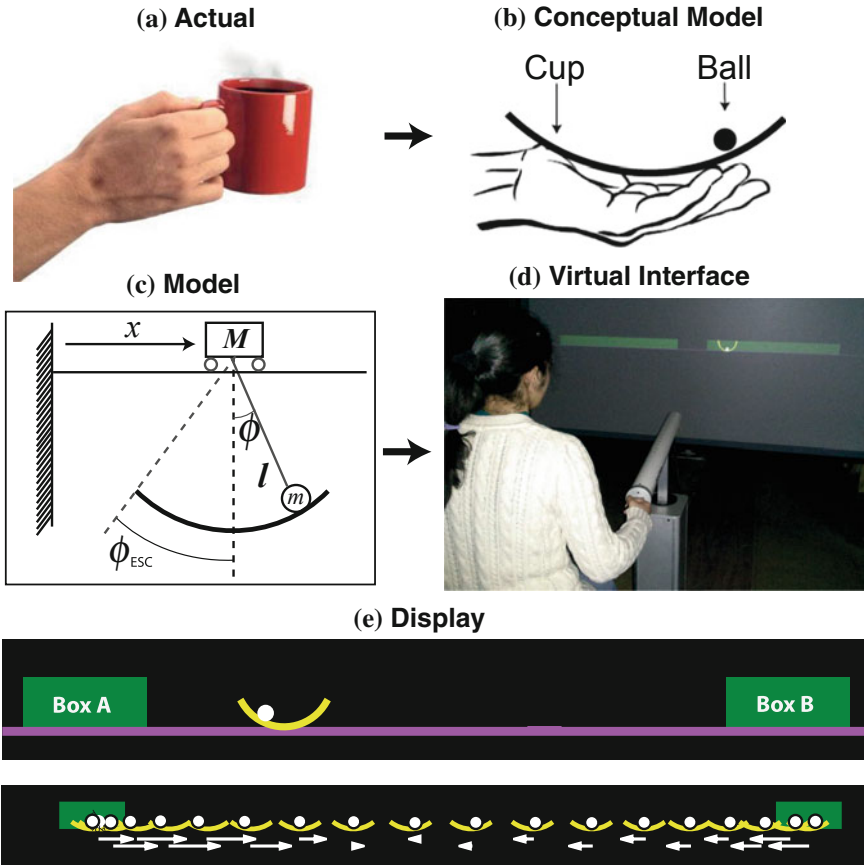


Fig. 10 Carrying a cup of coffee. **a** The model task. **b** The conceptual model: a 2D arc with a ball rolling inside. **c** Control model of the cart-and-pendulum. **d** Virtual implementation with the HapticMaster robot to control the cup in the horizontal direction. **e** The interactive screen display; the *green* rectangles specify the amplitude of the cup movement. The *lower panel* shows a sequence of moving cups with the *arrows* depicting the respective forces of cup and ball (Reproduced from [60])

617 a ball with point mass rolling in a cup, (3) the hand contact with the cup was reduced
 618 to a single point of interaction, (4) the cup transport was limited to a horizontal
 619 line (Fig. 10a–c). More precisely, the moving liquid is represented by a pendulum
 620 suspended to a cart that is translated in the horizontal x -direction. The pendulum is
 621 a point mass m (the ball) with a mass-less rod of length l with one angular degree of
 622 freedom θ . Subjects control the ball indirectly by applying forces to the cup, and the
 623 ball can escape if its angle exceeds the rim of the cup. The cup is a point mass M that
 624 moves horizontally. The hand moving the cup is represented by a horizontal force
 625 $F(t)$. Despite these simplifications, the model system retained essential elements of
 626 complexity: it is nonlinear and creates complex interaction forces between hand and

627 object. The equations of the system dynamics are:

$$\begin{aligned}
 628 \quad (m + M)\ddot{x} &= ml(-\ddot{\theta}\cos\phi + \dot{\theta}^2\sin\phi) + F(t) \\
 629 \quad l\ddot{\theta} &= -\ddot{x}\cos\theta - g\sin\theta
 \end{aligned}
 \tag{6}$$

631 where θ , $\dot{\theta}$, and $\ddot{\theta}$ are angular position, velocity, and acceleration of the ball/pendulum;
 632 x , \dot{x} , and \ddot{x} and are the cart/cup position, velocity, and acceleration, respectively; F
 633 is the force applied to the cup by the subject; g is gravitational acceleration. The
 634 model has four state variables x , \dot{x} , θ , $\dot{\theta}$ and the externally applied force $F(t)$ that
 635 determines the behavior of the ball and cup system. Hence, only one variable $F(t)$ is
 636 under direct control of the subject, but this is co-determined by the ball/pendulum
 637 interacting with the cart. These instantaneous interaction forces make the distinc-
 638 tion into execution and result variables significantly more complicated than in the
 639 previous two examples.

640 5.3 Virtual Implementation

641 The ball-and-cup system was implemented in a virtual environment. The cart and the
 642 pendulum rod was hidden, leaving only the ball visible. In addition, a semicircular
 643 arc with radius equal to was drawn on the screen so that the ball appeared to roll
 644 in the cup (Fig. 10d, e). Subjects manipulate the virtual cup-and-ball system via
 645 a robotic arm, which measures hand forces $F_{External}$ applied to the cup but also
 646 exerts forces from the virtual object onto the hand (HapticMaster, Motek [77]).
 647 ϕ and $\dot{\phi}$ were computed online and the ball force F_{Ball} was computed based on
 648 system equations such that the force that accelerated the virtual mass ($(m + M)$)
 649 was $F_{applied} = M\ddot{x} = F_{External} + F_{Ball}$. Two rectangular target boxes set the required
 650 movement distance and spatial accuracy (for more details see [23]).

651 5.4 Model Analysis and Hypothesis

652 The cup of coffee can be moved as a relatively short discrete placement to a target, or
 653 in a more continuous fashion, as for example carrying the cup while walking. A pre-
 654 vious study examined a single placement onto a target focusing on the discontinuous
 655 aspect of the task: the coffee can be spilled [23, 24]. Given the noise intrinsic to the
 656 neuromotor system and the fluctuations created by the extrinsic cart-and-pendulum
 657 system, avoiding failure became the core challenge when the task was to move as
 658 fast as possible. The “distance” from losing the ball was quantified by an energy
 margin, defined as the difference between the current energy state and the one where

the ball angle would exceed the rim angle. Results showed that this continuous metric sensitively captured performance quality and learning in healthy and also older subjects.

Here, we review another study that examined more prolonged interaction, where the nonlinear dynamics manifests its full complexity and, technically, displays chaos [41, 68]. To this end, the task instruction was to move the cup rhythmically between two very large targets leaving amplitude under-specified; the task-specified frequency defined the *result variable*. Movement strategies were fully described by the *execution variables* cup amplitude, frequency, and initial angle and velocity of the ball, $A, f, \theta_0, \dot{\theta}_0$. To derive hypotheses about the space of solutions, inverse dynamics analysis was conducted to calculate the force $F(t)$ required to satisfy the task. Numerical simulations were run for combinations of the scalar execution variables $A, f, \theta_0, \dot{\theta}_0$. To keep the number of simulations manageable, frequency f was fixed to the task-required frequency, and $\dot{\theta}_0$ was set to zero.

Figure 11 shows two example profiles generated by inverse dynamics calculations with two different initial ball states θ_0 ($\dot{\theta}_0 = 0$) that both result in a sinusoidal cup trajectory $x(t)$. The left profile $F(t)$ shows irregular unpredictable fluctuations for $\theta_0 = 0.4$ rad, while the right profile initialized at $\theta_0 = 1.0$ rad shows a periodic waveform with high regularity. To characterize the pattern of force profiles with respect to the cup dynamics, $F(t)$ was strobed at every peak of cup position $x(t)$. The marginal distributions of the strobed force values are plotted as a function of initial ball phase θ_0 in the bottom panel. This input-output relation reveals a bifurcation diagram with a pattern similar to the period-doubling behavior of chaotic systems, indicating chaos in the cup-and-ball system.

5.5 Hypotheses for Human Control Strategies

It seems uncontested that controlling physical interaction requires “knowledge” and prediction of object dynamics. On the other hand, it is reasonable to doubt that the complex details of object dynamics are known or faithfully represented in an internal model. In chaotic dynamics, small changes in initial states can dramatically change the long-term behavior and, technically, lead to unpredictable solutions. Can or should internal models be able to represent this complex dynamics? To make this challenge more tractable for the neural control system we hypothesized that subjects seek solutions that render the object behavior more predictable to reduce computational effort and facilitate at least some prediction.

To quantify the concept of predictability of the object dynamics based on the human’s applied force, we computed mutual information MI between the applied force and the kinematics of the cup, i.e. long-term predictability of the object’s dynamics [9]. MI is a nonlinear correlation measure defined between two probability density distributions and measures the information shared by two random variables, $F(t)$ and the kinematics of the cup $x(t)$:

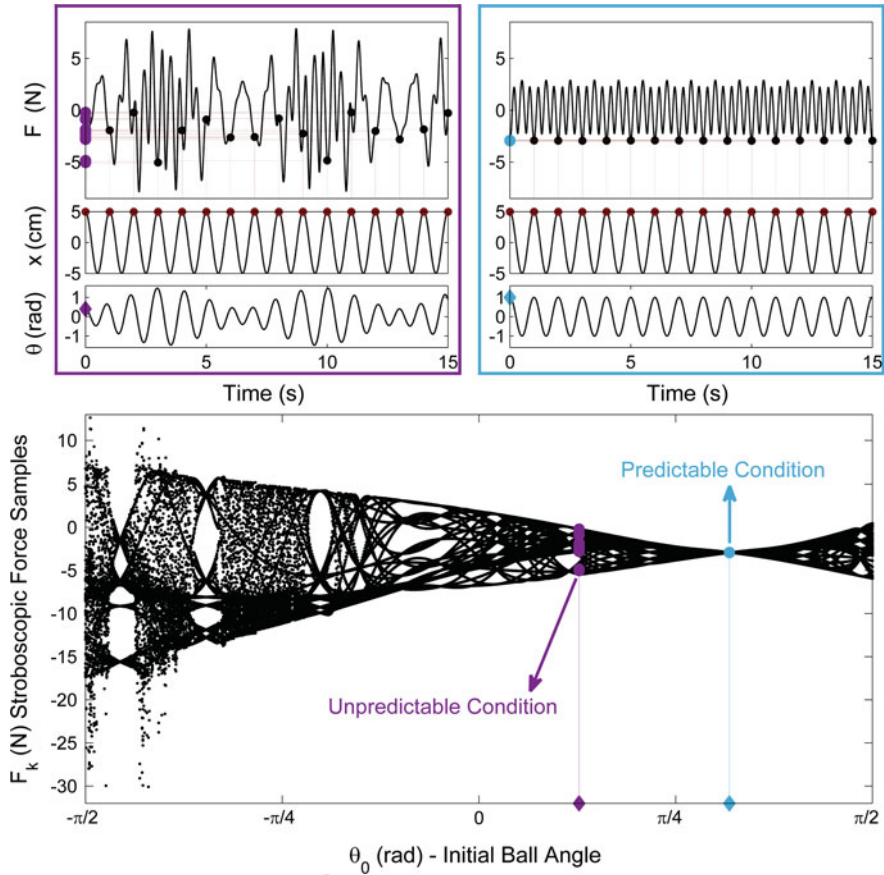


Fig. 11 Inverse dynamics simulations of the cart-and-pendulum model. *Top panels* show two different simulation runs with different initial ball angles θ_0 , requiring a complex and a relatively simple input force (*top row*). Strobing force values at maxima of the cup profile x and plotting the marginal distributions against all ball angles renders the bifurcation-like diagram (Reproduced from [41])

699

$$MI(x, F) = \iint p(x, F) \log_e \frac{p(x, F)}{p(x)p(F)} dx dF \quad (7)$$

700

701

702

703

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705

706

MI presents a scalar measure of the performer’s strategy calculated at each point of the 4D result space spanned by $A, f, \theta_0, \dot{\theta}_0$. The higher MI , the more predictable the relation between force and object dynamics. Hence, we expected that subjects would seek strategies with high MI (*Hypothesis 1*, Fig. 12a). Predictability as a control priority had to be tested against alternative hypothesis. The experiments permitted testing two alternative control priorities: minimizing effort (*Hypothesis 2*, Fig. 12b) and maximizing smoothness (*Hypothesis 3*, Fig. 12c); both are commonly accepted and

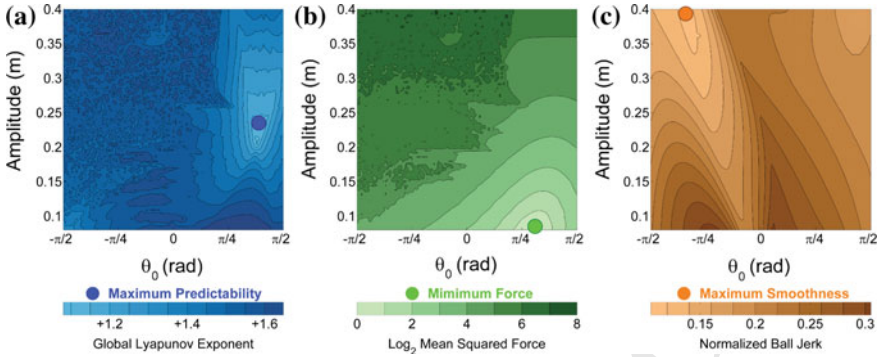


Fig. 12 Result space computed for three different hypothesized control priorities. The space is computed for different initial ball angles and cup amplitudes; frequency is set to 1 Hz, and ball velocity is set to zero. **a** Mutual information. **b** Effort defined as mean squared force over a given trial. **c** Smoothness or mean squared jerk defined over a given trial. The optimal strategy for each hypothesis is noted by the large dot (Reproduced from [41])

707 widely supported criteria in free unconstrained movements. To calculate the effort re-
 708 quired for each strategy, the Mean Squared Force of the force profile was calculated:

709
$$MSF = \frac{1}{nT} \int_0^{nT} F(t)^2 dt$$
, where n denoted the number of cycles and $T = 1/f$ the period

710 of each cycle. Mean Square Jerk was calculated as $MSJ = \frac{1}{T(\bar{\theta}_{max} - \bar{\theta}_{min})} \int_0^T |\ddot{\theta}|^2 dt$,

711 where the value was normalized with respect to ball jerk amplitude to make it di-
 712 mensionless [27]. Similar to MI , MSF -values were calculated for all strategies in 4D
 713 result space. To constrain the calculations, the initial value of the angular velocity
 714 $\dot{\theta}_0$ was set to zero, consistent with the experimental data. Figure 12 compares the
 715 corresponding predictions for MI , MSF , and MSJ . Color shades express the degree as
 716 explained in the legend. The large dots denote the points of maximum MI , minimum
 717 MSF and MSJ . Importantly, these predicted strategies are at very different locations
 718 in result space.

719 To test these hypotheses, equivalent measures had to be calculated from the
 720 experimental data to evaluate observed human strategies against the simulated result
 721 space. In contrast to the simulations, the experimental trajectories were not fully
 722 determined by initial values as online corrections were likely. Therefore, to attain
 723 better estimates of the execution variables from the experimental trajectories, esti-
 724 mates were extracted at each cycle k of the cup displacement x during each 40 sec
 725 trial (see Fig. 11); trial averages \bar{A} , \bar{f} , $\bar{\theta}_0$, $\bar{\dot{\theta}}_0$ served as correlates for the variables
 726 in the simulations. MI , MSF , and MSJ were calculated for each measured strategy
 727 \bar{A}_k , \bar{f}_k , $\bar{\theta}_k$, $\bar{\dot{\theta}}_k$.

5.6 Predictable Interactions

An experimental study provided first evidence that subjects indeed favored predictable solutions over those that minimized the expended force and smoothness [41]. Subjects performed rhythmic cup movements paced at the natural frequency of the pendulum, which corresponded to the anti-resonance of the coupled system. This facilitated the emergence of the system's nonlinear characteristics with chaotic solutions that maximized the challenge. Amplitude was free to choose and relative phase between ball and cup was also unspecified. Each subject performed 50 trials (40 s each). By choosing the cup amplitude and phase, subjects could manipulate interaction forces of different complexity and predictability.

The main experimental results are summarized in Fig. 13; the plot shows *MI* in shades of purple (lighter shades denote higher *MI*) and contours of selected values of *MSF* (green) from the simulations overlaid with the results from human subjects; each data point represents one trial (red). The data clearly show how subjects gravitated towards areas with higher *MI*, i.e. strategies with more predictable interactions, consistent with *Hypothesis 1*. The left panel shows individual trials pooled over all subjects; darker red indicates early practice and lighter red indicates late practice.

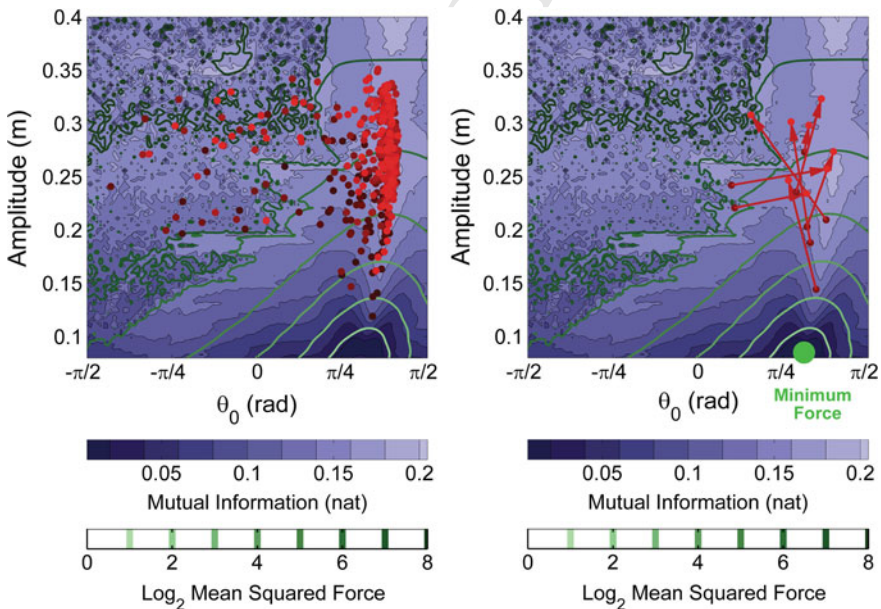


Fig. 13 Result space with Mutual Information as the result variable, shown by shades of purple. The left panel plots trial data from all 9 subjects showing that they converge to the area with highest MI. Each data point is one trial; darker color shades denote later in practice. The arrows in the right panel show each subject with initial trial values the start of the arrow and the final practice trial the tip of the arrow (Reproduced from [41])

745 The right panel shows the same data separated by subject: the red arrows mark how
 746 each subject's average strategy changed from early practice (mean of first 5 trials) to
 747 late practice (mean of last 5 trials). The majority of subjects switched from low- to
 748 high-predictability regions in the result space. Both figures also show that all subjects
 749 increased their movement amplitude, associated with an increase in overall exerted
 750 force. None of the subjects moved toward the minimum force strategy, nor towards a
 751 strategy with maximum smoothness (counter to Hypotheses 2 and 3). In fact, overall
 752 force exerted, or *MSF*, rather increased with practice.

753 5.7 Interim Summary

754 These results highlight that humans are sensitive to object dynamics and favor strate-
 755 gies that make interactions predictable. In the case shown, these predictable solutions
 756 were even favored over those with less effort. This is plausible because unpredictable
 757 interaction forces are experienced as disturbances that continuously require reactions
 758 and corrections. Knowing that in real life we carry a glass of wine without pay-
 759 ing much attention, more predictable strategies appear plausible. Analogous to the
 760 dynamically stable solutions in ball bouncing, predictable solutions may require
 761 fewer computations as they obviate error corrections. Given that in chaotic solu-
 762 tions small changes due to external or internal perturbations lead to unpredictable
 763 behavior, noise matters less in predictable solutions.

764 6 From Analysis to Synthesis: Dynamic Primitives 765 for Movement Generation

766 This brief overview of our research revealed potential control priorities or cost func-
 767 tions that humans may use to coordinate simple and complex interactions. Humans
 768 favor strategies that are sensitive to dynamics and stability, that exploit redundancy
 769 of the solution space to channel their intrinsic noise into task-irrelevant dimensions,
 770 and that exploit predictable solutions of potentially very complex task dynamics.
 771 The review also demonstrated what can be learnt from analysis of human data in
 772 conjunction with mathematical understanding of the task and its solution space. The
 773 only assumption is that the dynamics and stability properties of the task are funda-
 774 mental and determine "opportunities" and "costs". The known solution space serves
 775 as reference to evaluate human movement.

776 The task-dynamic approach as outlined is analytic and largely agnostic about
 777 details of the controller. This contrasts with other research in computational mo-
 778 tor neuroscience that starts with a hypothesized controller and then compares the
 779 predicted with the experimentally observed behavior. One recent prominent exam-
 780 ple for this direction is work that has sought evidence that the brain operates like an

781 optimal feedback controller [56, 74, 75]. Other control models include internal mod-
782 els with Kalman-filters or tapped-delay lines, to mention just a few [39]. Our approach
783 refrains from such assumptions directly borrowed from control theory; rather, we aim
784 to extract principles from human data with as few assumptions as possible. Never-
785 theless, the question of synthesis remains: what controller or control policy would
786 generate these strategies? While still largely speculative, our task-dynamic perspec-
787 tive presents a sound foundation for a generative hypothesis.

788 To begin, let's return to the initial pointer to the seemingly inferior features of
789 the human neuromotor system - the high degree of noise and the slow informa-
790 tion transmission. These features seem puzzling given the extraordinary dexterity
791 of humans that by far surpasses that of robots, at least to date. Therefore, the direct
792 translation of control policies that heavily rely on central control and feedback loops
793 may remain inadequate to achieve human dexterity. As mentioned earlier, the human
794 wetware with its compliant actuators and high dimensionality appears to provide
795 an advantage. Hence, lower levels of the hierarchical neuromotor system should be
796 given more responsibility. Consistent with our task-dynamic perspective, we have
797 therefore suggested that the biological system generates movements via dynamic
798 primitives, defined over the high-dimensional nonlinear neuromotor system [26, 28,
799 45, 50, 51, 59, 65]. We propose that the human neuromotor system exploits attrac-
800 tors states, defined over both the neural and mechanical nonlinear system. If the
801 neuromotor system is parameterized to settle into such stable states, central control
802 may only need to occasionally intervene. In principle, nonlinear autonomous sys-
803 tems have three possible stable attractor states: fixed point, limit cycle, and chaotic
804 attractors. Putting chaotic attractors aside for now, we proposed fixed-point and limit
805 cycle attractors for primitives.

806 The two main stable attractors fixed points and limit cycles directly map onto dis-
807 crete and rhythmic movements. To understand discrete movements such as reaching
808 to a target as convergence to a stable end state is not completely new. Equilibrium-
809 point control was first posited by Feldman for simple position control [14, 15].
810 Numerous subsequent studies, both behavioral and neurophysiological, have given
811 evidence for attractive properties in reaching behavior [4, 20, 25, 36]. This work has
812 widened to include a virtual trajectory, even though details are still much contested.
813 For rhythmic behavior a similar host of experimental and modeling studies have
814 presented support for stable limit cycle dynamics. For example, bimanual rhythmic
815 finger movements showed transitions from anti-phase to in-phase coordination that
816 bear the hallmarks of nonlinear phase transitions in coupled nonlinear oscillators
817 [22, 33]. Our own work has shown how extremely simple oscillator models can
818 account for synchronization in bimanual rhythmic coordination, including subtle
819 phase differences between oscillators with different natural frequencies [63, 71, 72].
820 Several different oscillator models have been developed that produce autonomous
821 oscillations to represent central pattern generators in the spinal cord of invertebrates
822 [31, 45]. Support for the distinction between rhythmic and discrete movements also
823 came from a neuroimaging study [54]. Brain activation revealed that in rhythmic
824 movements only primary motor areas were activated, while significantly more areas
825 were needed to control discrete movements.

826 In an attempt to synthesize this evidence from largely disparate research groups,
 827 our own research made first forays into combining the two types of building blocks.
 828 Playing piano is after all a combination of complex rhythmic finger movements
 829 combined with reaches across the keyboard. Note that in principle, optimal feedback
 830 control could also achieve such movements, including those with dynamic stability.
 831 In fact, there is no inherent limit to what optimal feedback control may achieve.
 832 It is this omnipotence that contrasts with the well-known coordinative limitations
 833 that may reveal features of the human controller. Beyond “patting your head while
 834 rubbing your stomach”, research has revealed that rhythmic bimanual actions tends
 835 to settle into in-phase and anti-phase coordination [34, 72], humans avoid moving
 836 very slowly [3, 78], and the 2/3 power law in handwriting and drawing may reveal
 837 intrinsic geometry or other limitations [18, 52]. Several modeling and experimental
 838 studies showed the possibilities and limitations of combining two dynamic primitives.
 839 Wiping a table rhythmically, while translating the hand across the table revealed that
 840 rhythmic and discrete elements cannot be combined arbitrarily [64, 65].

841 However, research is still far from having generated conclusive evidence that
 842 dynamic motion primitives underlie observed behavior. More specifically,
 843 interactions with objects cannot be addressed with the two primitives alone. There-
 844 fore, recently Hogan and myself argued that impedance is needed as a third dy-
 845 namic primitive to enable the system to interact with objects and the environment
 846 [28, 29]. Combining discrete and rhythmic primitives with impedance in an equiv-
 847 alent network is a first proposal on how humans may interact with objects in the
 848 environment. More details and first theoretical developments can be found in the
 849 chapter of Hogan in the same volume. With these theoretical efforts under way, also
 850 further complementary empirical work is needed. The challenge for the future is to
 851 combine analysis and synthesis. How can dynamic primitives be employed to pour
 852 a glass of wine?

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Chapter 13

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